

# Medical Image De-Noising Schemes using Wavelet Transform with Fixed form Thresholding

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**Abstract**—Medical Imaging is currently a hot area of bio-medical engineers, researchers and medical doctors as it is extensively used in diagnosing of human health and by health care institutes. The imaging equipment is the device, which is used for better image processing and highlighting the important features. These images are affected by random noise during acquisition, analyzing and transmission process. This condition results in the blurry image visible in low contrast. The Image De-noising System (IDS) is used as a tool for removing image noise and preserving important data. Image de-noising is one of the most interesting research areas among researchers of technology-giants and academic institutions. For Criminal Identification Systems (CIS) & Magnetic Resonance Imaging (MRI), IDS is more beneficial in the field of medical imaging. This paper proposes an algorithm for de-noising medical images using different types of wavelet transform, such as Haar, Daubechies, Symlets and Bi-orthogonal. In this paper noise image quality has been evaluated using filter assessment parameters like Peak Signal to Noise Ratio (PSNR), Mean Square Error (MSE) and Variance, It has been observed to form the numerical results that, the presentation of proposed algorithm reduced the mean square error and achieved best value of peak signal to noise ratio (PSNR). In this paper, the wavelet based de-noising algorithm has been investigated on medical images along with threshold.

**Keywords**—Image De-noising System; GUI De-noised image; Code De-noised image; Wavelet transform; Soft and Hard Threshold

## I. INTRODUCTION

Recently most of human-assisted computer applications rely on the use of digital image processing techniques, such as magnetic resonance imaging (MRI), criminal identification systems (CIS), agricultural and biological research (ABR). The term image de-noising is the best tool used in these applications, where it aims at remove the noise and retain important image features as much as possible. The use of medical imaging (MRI) in diagnosis has been greatly accepted for its non-sensitive features, low cost, the ability of constructing real-time image with improved property[1], [2]. During image acquisition and transmission, it has been usually observed that random noise always occurs at another end. So this noise causes problems such as a blurred vision of images, which reduce the visuality of low-contrast articles.

Therefore, it is not easy for the medical doctors to examine the abnormalities in human in the invisible image. The process of removing noise is necessary in most medical imaging equipments for the purpose of enhancing miniatures that may be concealed in the data [3][4].

## II. WAVELET TRANSFORM

This wavelet transform is alike to Windowed Fourier Transform (WFT), but the merit function is totally different. The main difference between the Window Fourier Transform and wavelet lies in the signal analysis; The WFT breaks down the signal into cosines and sines and, namely, the functions are restrained in Fourier space. On the contrary, functions that are utilized in the wavelet transform are confined in the real space and the Fourier space. Commonly, the Continuous Wavelet Transform (CWT) is containing different parameters which are derived from Fourier analysis transform and mother wavelet transform. The equation (1) describes the parameter  $\gamma(s, \tau)$  is a wavelet coefficient with scale  $s$  and time  $\tau$ , and the function  $f(t)$  is define as the time series wherethe certain function is  $\psi_{s,\tau}^*$  defines a complex conjugate of wavelet with scale and times,  $\tau$ . [5][6].

$$\gamma(s, \tau) = \int f(t) \psi_{s,\tau}^*(t) dt \quad (1)$$

Wavelets have been considered recently as a strong tool for de-noising image. The individual wavelet makes an image into a group of coefficients that compose a multi-scale model of the image. The distinct wavelet transform of signal expressed as  $x(n)$  is calculated by making it go through a low pass filter with impulse response  $g(n)$  as long as given an approximation coefficient. The signal is breaks down concurrently by the use of a high pass filter  $h(n)$ , while gives details coefficients. These filters are named as Quadratic Mirror Filters. Because the half of frequencies of the signal is taken out, the sample of the filter outputs are reduced by equation (2)&(3).

$$Y_{low}[k] = \sum_n x[n].g[2k - n] \quad (2)$$

$$Y_{high}[k] = \sum_n x[n].g[2k - n] \quad (3)$$

Image is a 2-dimensional signal, and we use  $x(N, M)$  to represent it. Firstly each row is filtrated and then down-sampled to get two images represented by  $(N, M/2)$ , secondly every column is filtrated and down-sampled to get four sub bands named as HH, HL, LH and LL Therefore, in case of two dimensions, one 2-D scaling function and three 2-D wavelet functions are generated.

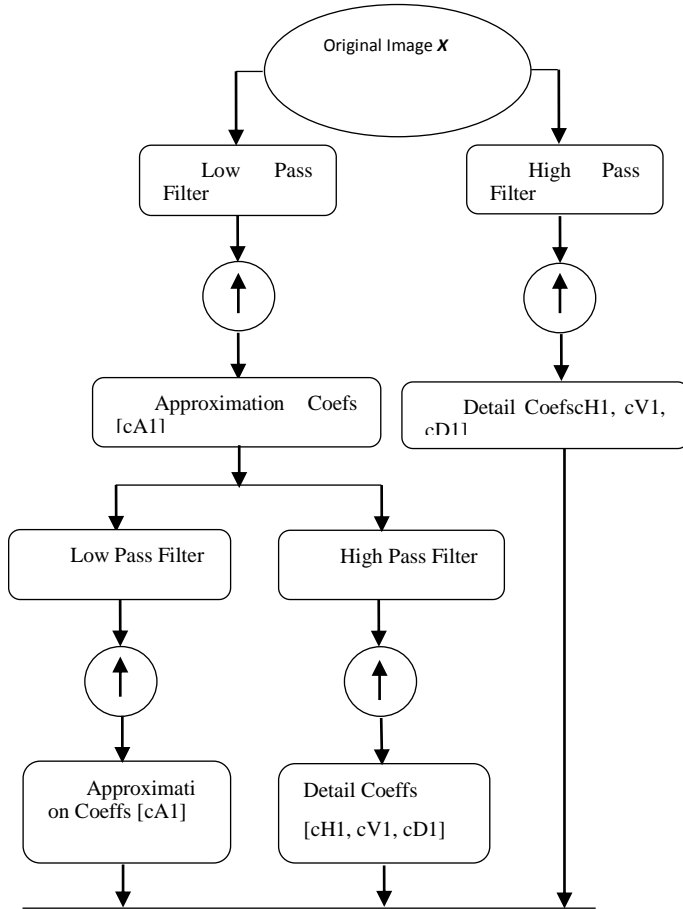


Fig. 1. The 2D discrete wavelet decomposition

The variable CA1, CD1, CH1 and CV1 stand for approximation coefficient, diagonal detail coefficient, horizontal detail coefficient and vertical detail coefficient.

At level two approximation sub-band LL is then decomposed into four components, the performance can be progressed all the same for another three levels. LL has strength concentration for low pass and HH sub-band for high-frequency constituents. Rebuilding can be performed by IDWT (Inverse Discrete Wavelet Transform) to obtain the de-noised image [7] [8].

The process of 2D discrete wavelet decomposition has been depicted in figure.1, which describes the main steps for de-noising. The process starts from image decomposition, up-sampling and down-sampling until the reconstruction of four sub band coefficients are obtained for original image [9][10].

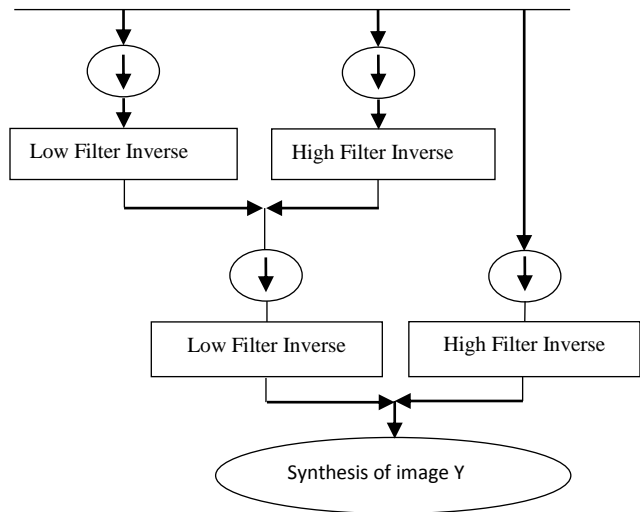


Fig. 2. The 2D discrete wavelet reconstruction

Here, figure.2 illustrates; brain image reconstruction from three-level decomposition. We can see the wavelet decomposition process can be seen by consecutive approximations being decomposed successfully. In figure three the original medical image shows decomposition into many elements with lower-resolution.

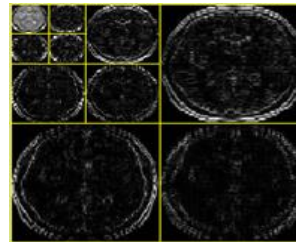


Fig. 3. Wavelet three-level decomposition of brain image

### III. PROPOSED ALGORITHM FOR DE-NOISING

The purpose of this paper is the de-noising of medical image of the brain using different types of wavelets, such as Haar, db10, sym3 and bior3.7 wavelet. Our contribution in this paper is that good results are obtained when applying fixed form threshold in terms of soft and hard threshold algorithm. To evaluate the proposed algorithm, several parameters are used such as Peak Signal to Noise Ratio (PSNR), Mean Square Error (MSE) and Variance. Numerical results show the validity of proposed algorithm. The mean square error is reduced, while a peak signal to noise ratio (PSNR) is achieved.

#### A. Image De-noising Algorithm

There are three steps of de-noising procedure described as follows:

Wavelet decomposition level Pick a level (level-3). Calculate the wavelet decomposition of the noisy image at level 3. The wavelet produces all the coefficients, from the wavelet analysis process.

Threshold detail coefficients: a threshold is chosen for level 3 and soft thresholding is applied to the detail coefficients. If the wavelet coefficients are larger than the threshold value, those coefficients are left unaltered. If they are small than threshold, they are restrained.

Reconstruct wavelet coefficients based on level 3 of wavelet transform. Then, transform detailed coefficients from level 3 to level 1.

### B. Thresholding Parameter

In this part parameters are formulated and used for de-noising.

#### 1) Noise variance

Apply a fixed form thresholding algorithm to the wavelet coefficients. In fixed form, the noise variance is calculated using the median of absolute deviation of the transform coefficient of all three levels; the (MAD) is given by equation (4).

$$\sigma_n^2 = \frac{\text{median}(\text{abs}(x_{ij}))^2}{0.6745} \quad (4)$$

#### 2) Threshold Parameter

The threshold ( $T_h$ ) is a threshold parameter applied to wavelet coefficients of a noisy image. Where M is number of pixels in the image, and S is the noise variance and the threshold is given by equation (5).

$$Th = \sigma \sqrt{2 \log M} \quad (5)$$

Hard thresholding is a keep or kill the wavelet coefficients compared with threshold parameter. The threshold is deducted from any coefficient that is larger than the threshold. This process makes the time series move toward zero.

### C. Evaluation Parameters

In this part evaluation parameters are discussed.

#### 1) Mean Square Error (MSE)

The MSE estimate the quality alteration between the GUI de-noised image (X) and code demised image (Y), the average of the squared image is given in equation (6).

$$MSE = \frac{1}{mn} \sum_{i=0}^{m-1} \sum_{j=0}^{n-1} [Y(i, j) - X(i, j)]^2 \quad (6)$$

#### 2) Peak Signal to Noise Ratio (PSNR)

The PSNR represents the size of the error in relation to the peak value of the signal rather than the size of the error in relation to the average squared value of the signal. It is computed with the size of the error in relation to the average squared value of the signal. PSNR is greater for a better-transformed image and smaller for a poorly transformed image. PSNR calculates image fidelity, i.e., intimately the transformed image looks like the initial image, the PSNR exhibited in equation (7).

$$PSNR = 10 \log_{10} \left[ \frac{S^2}{mse} \right] \quad (7)$$

## IV. RESEARCH METHODOLOGY

The experiments in this paper have been conducted on two medical images; of Brain with different size. The first image is a brain medical image with size [204x204], the second image is a brain medical image with size [150x150]; Different types of wavelet transform have been applied respectively (haar, db10, sym3, and bior3.7) for these two images to generate de-noised image. After applying wavelet, (CA) approximation and (CD) details coefficient at three levels of decomposition process have been generated. These coefficients represented in vector [C,S] such as [CD1, CD2, CA3, CD3]. After each level consists of horizontal, vertical and diagonal coefficients, de noising image is achieved. As there are many threshold levels but in this paper, fixed form soft threshold for three levels of decomposition process have been selected because it will give best threshold value. Here un-scaled white noise is added to the original image to generate a de-noising image in GUI (Graphical User Interface). At the first stage, the original image is compared with the GUI de-noising image. for the same scheme, MATLAB codes are written to compare the original image using hard threshold with the image de-noising generated code. At the later stage the GUI de-noising image is compared with the image de-noising generated code along with MSE and PSNR parameter.

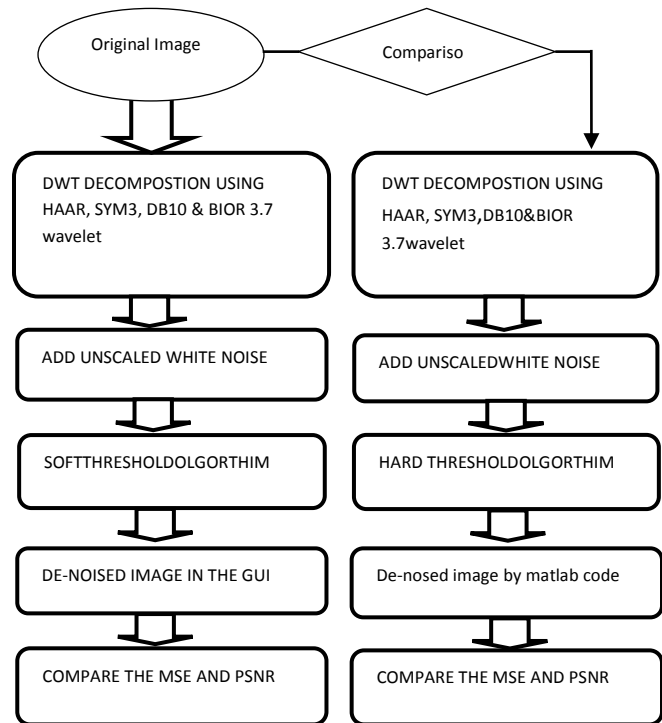


Fig. 4. De Nosing Comparison Algorithm Model

## V. RESULTS AND DISCUSSION

Here Fig.5 illustrates the initial medical image of brain image. Fig 6&7 depicts the de-noising images generated in GUI and MATLAB Code.

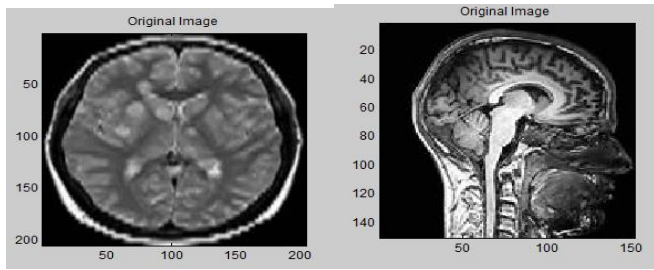


Fig. 5. The original of two brain images

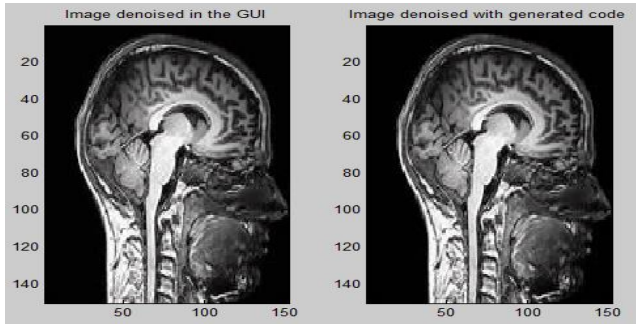


Fig. 6. The De-noised of first brain image

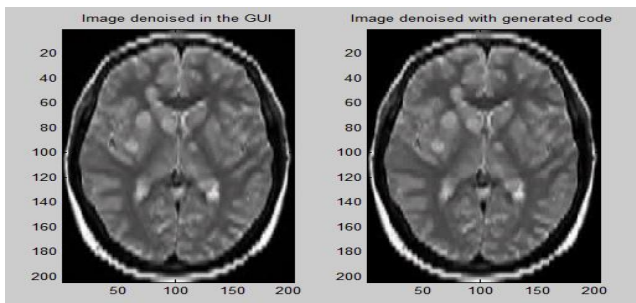


Fig. 7. The De-noised second brain image

The Performance evaluation of de-noising image can be observed in the tables 1 & 2. From the relationship of the peak signal and mean square to the noise ratio, here it can be observed from Table 1 & 2 that the MSE measurements in the GUI generated de-noising image are smaller than the measurements in the code generated de-noising image in all wavelet families. It reveals that the mean square error of the initial image in GUI is less than the hard threshold generated code of the original image. That is because of the image size.

TABLE I. PERFORMANCE EVALUATION OF GUI METHOD FOR DIFFERENT THRESHOLDING IN TERM OF MSE, PSNR FOR TWO DIFFERENT BRAIN IMAGES

Various image	Wavelet package	Soft Threshold Method		Hard Threshold Method	
		MSE	PSNR	MSE	PSNR
Brain image with size (150x150)	haar	0.8436	48.2026	3.4461	41.7699
	db10	0.8697	48.2200	3.2437	41.6534
	sym3	0.7360	48.2309	3.2600	41.8367
	bior3.7	0.6589	48.2433	2.6374	41.9085
Brain	haar	0.8280	48.1395	4.3343	38.9221

image with size (200x200)	db1	0.8	48.1	5.5	39.9
	sym3	0.7062	48.1809	4.8423	40.2849
	bior3.7	0.6612	48.2085	3.4412	42.2548

TABLE II. PERFORMANCE EVALUATION OF MATLAB CODE METHOD FOR DIFFERENT THRESHOLDING IN TERM OF MSE, PSNR FOR TWO DIFFERENT BRAIN IMAGES

Various Images	Wavelet package	Soft Threshold Method		Hard Threshold Method	
		MSE	PSNR	MSE	PSNR
Brain image with size (150x150)	haar	0.9080	48.1395	7.3343	38.9221
	db10	0.9395	48.3085	4.5580	39.9631
	sym3	0.8962	48.3709	5.8423	42.2849
	bior3.7	0.7212	48.6485	2.4412	44.2548
Brain image with size (200x200)	Haar	0.9312	47.2095	9.4413	38.3264
	db10	0.9122	47.2526	7.2052	40.5231
	sym3	0.9482	47.3929	8.2311	41.4223
	bior3.7	0.7551	47.5425	3.1220	43.1253

Fig. 8 & 9 illustrates the relationship of MSE & PSNR of four wavelet families for brain de-noising medical image. Here it can be observed that bior3.7 wavelet has better results than the other wavelet families used in this paper for image de-noising.

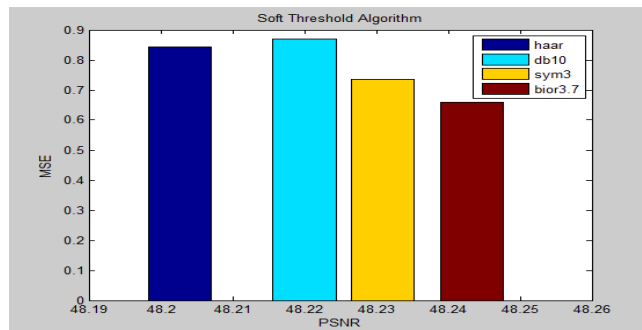


Fig. 8. The histogram of GUI method using Soft Threshold Algorithm for Brain de-noising image

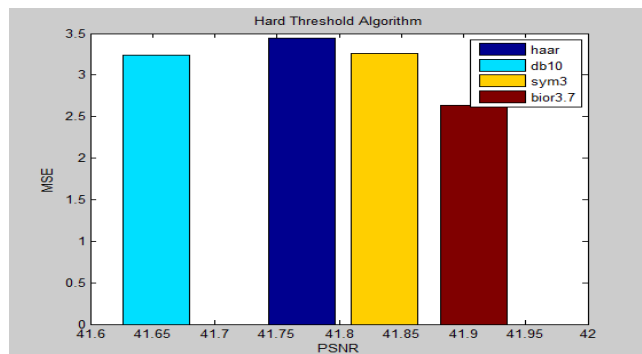


Fig. 9. The histogram of GUI method using Hard Threshold Algorithm for Brain de-noising image

Fig. 10 & 11 illustrates the relationship of MSE & PSNR of four wavelet families for the brain de-noising medical image. Here it can be observed that bior3.7 wavelet has better results than the other wavelet families used in this paper for image de-noising.

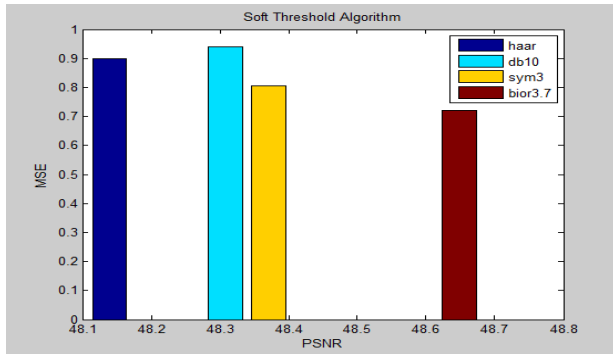


Fig. 10. The histogram of MATLAB code method using Hard Threshold Algorithm for brain de-noising image

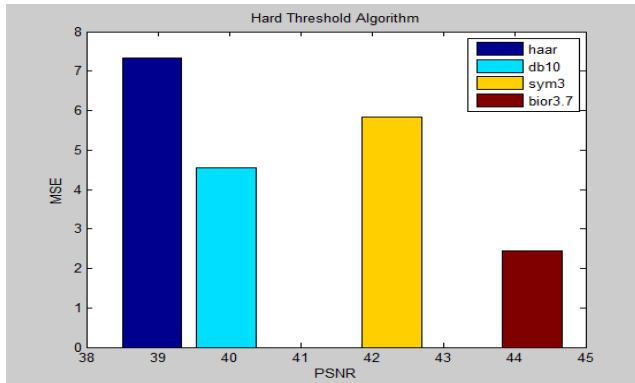


Fig. 11. MATLAB code method using Hard Threshold Algorithm for brain de-noising image

Fig. 12& 13 illustrates the relationship of MSE & PSNR of four wavelet families for the brain de-noising medical image. Here it can be observed that bior3.7 wavelet has better results than the other wavelet families used in this paper for image de-noising.

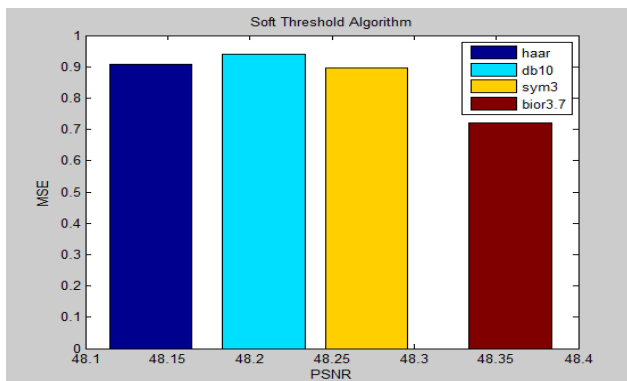


Fig. 12. The histogram of GUI method using Soft Threshold Algorithm for brain de-noising image

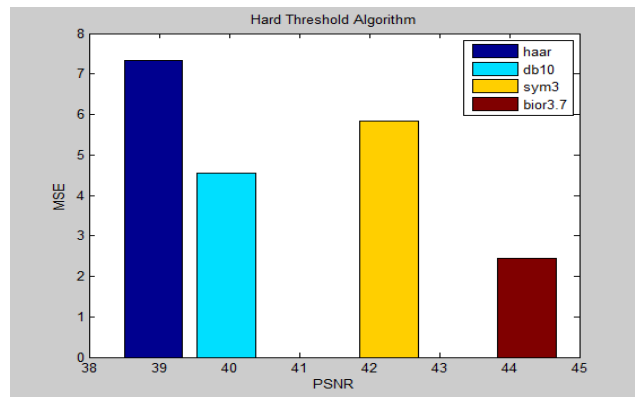


Fig. 13. The histogram of GUI method using Hard Threshold Algorithm for brain de-noising image

Fig. 14& 15 illustrates the relationship of MSE & PSNR of four wavelet families for the de-noising medical image. Here it can be observed that bior3.7 wavelet has better results than the other wavelet families used in this paper for image de-noising.

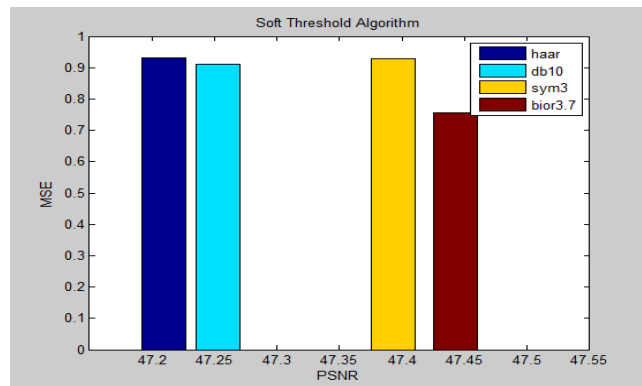


Fig. 14. The histogram of MATLAB code method using Hard Threshold Algorithm for Brain de-noising image

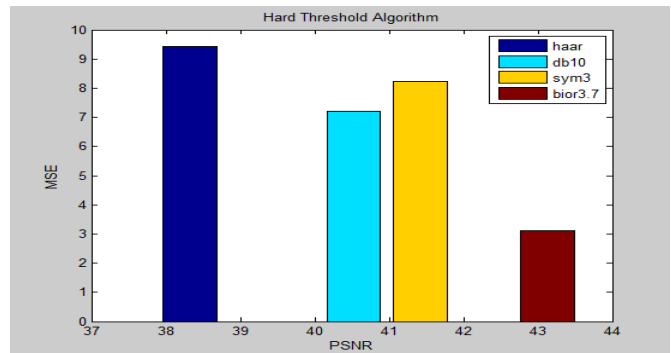


Fig. 15. The histogram of MATLAB code method using Hard Threshold Algorithm for Brain de-noising image

## VI. CONCLUSIONS

In all images, noise is the main problem, and one has to nip this problem in the bud for better results.

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De-noising is very crucial especially in medical science. In this paper, removing the un-scaled white noise added to original medical images has been presented. The new algorithm has been proposed for De-noising brain medical images. The proposed new algorithm on the basis of the wavelet transform is observed to be a more competent method in image de-noising especially for removing un-scaled white noise. Qualitative and quantitative analysis results reveal that the proposed algorithm reduces the mean square error (MSE) of different images with different sizes using different wavelet families for hard and soft threshold. Experiments represent that, the bi-orthogonal wavelet is a more efficient method than other wavelet families discussed in this paper, such as Haar, Daubechies, and Symlets because it gave better results with mean square error (MSE) in soft and hard threshold. Efficient de-noising values in a soft threshold algorithm are generated in GUI. Because of difference in image sizes, hard threshold algorithm generated code values were observed as larger in case of the brain medical image. Results reveal that bi-orthogonal wavelet shows the best results with parameter MSE and PSNR. At the later stages one can work precisely on MSE and PSNR measurements for both soft and hard thresholds for getting de-noised medical images.

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